

Functional reorganization of brain networks across the human menstrual cycle

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Key Words: sex hormones, estrogen, progesterone, menstrual cycle, fMRI, functional connectivity, brain networks, resting state

Abstract

1
2 Densely sampling the individual connectome could transform our understanding of the
3 functional organization of the human brain. The brain is an endocrine organ, sensitive to
4 cyclic changes in hormone production. However, the influence of sex hormones on the
5 brain's intrinsic network architecture is largely unknown. Here, we examine the extent to
6 which endogenous fluctuations in sex hormones alter functional brain networks at rest in
7 a woman over 30 consecutive days. Time-synchronous analyses illustrate estrogen and
8 progesterone's widespread influence on cortical dynamics throughout the cycle. Time-
9 lagged analyses examined the temporal flow of these relationships and reveal estrogen's
10 ability to drive connectivity across major functional networks, including the Default
11 Mode and Dorsal Attention Networks, whose hubs are densely populated with estrogen
12 receptors. These results reveal the rhythmic nature of brain network reorganization
13 across the human menstrual cycle. Considering the hormonal milieu is critical for fully
14 understanding the intrinsic dynamics of the human brain.

Introduction

15
16 The brain is an endocrine organ whose day-to-day function is intimately tied to the action
17 of neuromodulatory hormones¹⁻⁴. Yet, the study of brain-hormone interactions in human
18 neuroscience has often been woefully myopic in scope: the classical approach of
19 interrogating the brain involves collecting data at a single time point from multiple
20 subjects and averaging across individuals to provide evidence for a
21 hormone-brain-behavior relationship. This cross-sectional approach obscures the rich,
22 rhythmic nature of endogenous hormone production. A promising trend in network
23 neuroscience is to flip the cross-sectional model by tracking small samples of individuals
24 over timescales of weeks, months, or years to provide insight into how biological,
25 behavioral, and state-dependent factors influence intra- and inter-individual variability in
26 the brain's intrinsic network organization⁵⁻⁷. Neuroimaging studies that densely sample
27 the individual connectome are beginning to transform our understanding of the dynamics
28 of human brain organization. However, these studies commonly overlook sex steroid
29 hormones as a source of variability—a surprising omission given that sex hormones are
30 powerful neuromodulators that display stable circadian, infradian, and circannual
31 rhythms in nearly all mammalian species. In the present study, we illustrate robust,
32 time-dependent interactions between the sex steroid hormones 17β -estradiol and
33 progesterone and the functional network organization of the brain over a complete
34 menstrual cycle, offering compelling evidence that sex hormones drive widespread
35 patterns of connectivity in the human brain.

36 Converging evidence from rodent¹¹²³, non-human primate⁹¹⁰, and human
37 neuroimaging studies¹¹⁻¹⁶ has established the widespread influence of 17β -estradiol and
38 progesterone on regions of the mammalian brain that support higher level cognitive
39 functions. Estradiol and progesterone signaling are critical components of cell survival
40 and plasticity, exerting excitatory and inhibitory effects that are evident across multiple
41 spatial and temporal scales⁴³. The dense expression of estrogen and progesterone
42 receptors (ER; PR) in cortical and subcortical tissue underscores the widespread nature of
43 hormone action. For example, in non-human primates ~50% of pyramidal neurons in
44 prefrontal cortex (PFC) express ER¹⁰ and estradiol regulates dendritic spine proliferation
45 in this region³. In rodents, fluctuations in estradiol across the estrous cycle enhance
46 spinogenesis in hippocampal CA1 neurons and progesterone inhibits this effect¹.

47 During an average human menstrual cycle, occurring every 25-32 days, women
48 experience a ~12-fold increase in estradiol and an ~800-fold increase in progesterone.
49 Despite this striking change in endocrine status, we lack a complete understanding of how
50 the large-scale functional architecture of the human brain responds to rhythmic changes
51 in sex hormone production across the menstrual cycle. Much of our understanding of
52 cycle-dependent changes in brain structure¹¹⁷ and function¹⁸⁻²⁰ comes from rodent studies,
53 since the length of the human menstrual cycle (at least 5× longer than rodents') presents
54 experimental hurdles that make longitudinal studies challenging. A common solution is to
55 study women a few times throughout their cycle, targeting stages that roughly correspond
56 to peak/trough hormone concentrations. Using this 'sparse-sampling' approach, studies

57 have examined resting-state connectivity in discrete stages of the cycle^{13,14,21-23}, however,
58 some of these findings are undermined by inconsistencies in cycle staging methods, lack
59 of direct hormone assessments, or limitations in functional connectivity methods.

60 In this dense-sampling, deep-phenotyping study, we assessed brain-hormone
61 interactions over 30 consecutive days representing a complete menstrual cycle. Our
62 results reveal that intrinsic functional connectivity is influenced by hormone dynamics
63 across the menstrual cycle at multiple spatiotemporal resolutions. Estradiol and
64 progesterone conferred robust time-synchronous and time-lagged effects on the brain,
65 demonstrating that intrinsic fluctuations in sex hormones drive changes in the functional
66 network architecture of the human brain. Together, these findings provide insight into
67 how brain networks reorganize across the human menstrual cycle and suggest that
68 consideration of the hormonal milieu is critical for fully understanding the intrinsic
69 dynamics of the human brain.

70 Results

71 A healthy, naturally-cycling female (author L.P.; age 23) underwent venipuncture and MRI
72 scanning for 30 consecutive days. The full dataset consists of daily mood, diet, physical
73 activity, and behavioral assessments, task-based and resting-state fMRI, structural MRI,
74 and serum assessments of pituitary gonadotropins and ovarian sex hormones.
75 Neuroimaging data, code, and daily behavioral assessments will be publicly accessible
76 upon publication.

77 **Endocrine assessments**

78 Analysis of daily sex hormone (by liquid-chromatography mass-spectrometry; LC-MS)
79 and gonadotropin (by chemiluminescent immunoassay) concentrations confirmed the
80 expected rhythmic changes of a typical menstrual cycle, with a total cycle length of 27
81 days. Serum levels of estradiol and progesterone were lowest during menses (day 1-4) and
82 peaked in late follicular (estradiol) and late luteal (progesterone) phases (**Fig. 1; Table 1**).
83 Progesterone concentrations surpassed 5 ng/mL in the luteal phase, signaling an ovulatory
84 cycle.

85 **Time-synchronous associations between sex hormones and** 86 **whole-brain functional connectivity**

87 To begin, we tested the hypothesis that whole-brain functional connectivity at rest is
88 associated with intrinsic fluctuations in estradiol and progesterone in a *time-synchronous*
89 (i.e. day-by-day) fashion. Based on the enriched expression of ER in PFC¹⁰, we predicted
90 that the Default Mode, Frontoparietal Control, and Dorsal Attention Networks would be
91 most sensitive to hormone fluctuations across the cycle. For each session, the brain was
92 parcellated into 400 cortical regions from the Schaefer atlas²⁴ and 15 subcortical regions
93 from the Harvard-Oxford atlas (**Fig. 2c**). A summary time-course was extracted from each
94 parcel, data were temporally-filtered using a maximal overlap discrete wavelet transform
95 (scales 3-6; ~ 0.01 – 0.17 Hz), and 415×415 functional association matrices were constructed
96 via magnitude-squared coherence (FDR-thresholded at $q < .05$; see **Online Methods** for a
97 full description of preprocessing and connectivity estimation). Next, we specified edgewise

98 regression models, regressing coherence against estradiol and progesterone over the 30
99 days of the study. All data were Z -scored prior to analysis and models were thresholded
100 against empirical null distributions generated through 10,000 iterations of nonparametric
101 permutation testing. Results reported below survived a conservative threshold of $p < .001$.

102 We observed robust increases in coherence as a function of increasing estradiol across
103 the brain (**Fig. 2a**). When summarizing across networks (computing the mean association
104 strength across network nodes, where strength was defined per graph theory as the sum
105 of positive and negative edge weights linked to each node, independently), components
106 of the Temporal Parietal Network had the strongest positive associations on average,
107 as well as the most variance (**Fig. 2d**). With the exception of Subcortical nodes, all
108 networks demonstrated some level of significantly positive association strength (95%
109 CIs not intersecting zero). We observed a paucity of edges showing inverse associations
110 (connectivity decreasing while estradiol increased), with no networks demonstrating
111 significantly negative association strengths on average (**Fig. 2d**). These findings suggest
112 that edgewise functional connectivity is primarily characterized by increased coupling as
113 estradiol rises over the course of the cycle.

114 Progesterone, by contrast, yielded a widespread pattern of inverse association across
115 the brain, such that connectivity decreased as progesterone rose (**Fig. 2b**). Most networks
116 (with the exception of the Salience/Ventral Attention and SomatoMotor Networks) still
117 yielded some degree of significantly positive association over time; however, the general
118 strength of negative associations was larger in magnitude and significantly nonzero across

119 all networks (**Fig. 2d**). Together, these results align with animal models suggesting
120 excitatory and inhibitory roles for estradiol and progesterone, respectively, manifested
121 here as predominant increases and decreases in functional connectivity across the cycle.

122 **Time-lagged associations between estradiol and** 123 **whole-brain functional connectivity**

124 We then employed time-lagged methods from dynamical systems analysis to further
125 elucidate the influence of hormonal fluctuations on intrinsic functional connectivity:
126 specifically, vector autoregression (VAR), which supports more directed, causal inference
127 than standard regression models. Here we chose to focus exclusively on estradiol for two
128 reasons: 1) the highly-bimodal time-course of progesterone confers a considerably longer
129 autocorrelative structure, requiring many more free parameters (i.e. higher-order models,
130 ultimately affording fewer degrees of freedom); and 2) progesterone lacks an appreciable
131 pattern of periodicity in its autocovariance with network timeseries, suggesting less
132 relevance for time-lagged analysis over a single cycle. In contrast, estradiol has a much
133 smoother time-course that is well-suited for temporal-evolution models such as VAR.

134 In short, VAR solves a simultaneous system of equations that predicts *current* states of
135 the brain and estradiol from the *previous* states of each. We report results from second-order
136 VAR models: thus, in order to predict connectivity or hormonal states on a given day of
137 the experiment, we consider their values on both the previous day (hereafter referred to
138 as ‘lag 1’) and two days prior (hereafter referred to as ‘lag 2’). See **Online Methods** for an
139 additional mathematical description. Ultimately, if brain variance over time is attributable

140 to previous states of estradiol, this suggests that temporal dynamics in connectivity may
141 be *driven* (in part) by fluctuations in hormonal states. Vector autoregressive models were
142 specified for each network edge; as before, all data were *Z*-scored and models were
143 empirically thresholded against 10,000 iterations of nonparametric permutation testing.
144 Surviving edges were significant at the $p < .001$ level.

145 When predicting edgewise connectivity states, a powerful disparity emerged between
146 the brain's autoregressive effects and the effects of estradiol. We observed vast, whole-
147 brain associations with prior hormonal states, both at lag 1 and lag 2 (**Fig. 3a**). Perhaps
148 most immediately striking, the sign of these brain-hormone associations inverts between
149 lags, such that it is predominantly positive at lag 1 and predominantly negative at lag
150 2—this holds for all networks when considering their nodal association strengths (**Fig. 3b**).
151 We interpret this as a potential regulatory dance between brain states and hormones over
152 the course of the cycle, with estradiol perhaps playing a role in maintaining both steady
153 states (when estradiol is low) and transiently-high dynamics (when estradiol rises). No
154 such pattern emerged in the brain's autoregressive effects, with sparse, low-magnitude,
155 and predominantly negative associations at lag 1 and lag 2 (**Supplementary Fig. 1**). The
156 flow of effect between estradiol and edgewise connectivity was partially unidirectional.
157 Previous states of coherence predicted estradiol across a number of edges, intersecting
158 all brain networks. This emerged at both lag 1 and lag 2; however, unlike the lagged
159 effects of estradiol on coherence, association strengths were predominantly negative at
160 both lags (**Supplementary Fig. 2**). Moreover—and importantly—none of the edges that

161 *predicted* estradiol were also significantly predicted *by* estradiol at either lag (i.e. there was
162 no evidence of mutual modulation for any network edge).

163 **Time-lagged associations between estradiol and** 164 **functional network topologies**

165 Given the findings above, we applied the same time-lagged framework to *topological states*
166 of brain networks in order to better capture the directionality and extent of brain-hormone
167 interactions at the network level. These states were quantified using common graph theory
168 metrics: namely, the *participation coefficient* (an estimate of *between-network* integration) and
169 *global efficiency* (an estimate of *within-network* integration). As before, all data were *Z*-scored
170 prior to analysis, and model parameters/fit were compared against 10,000 iterations of
171 nonparametric permutation testing. We focus on significant network-level effects below,
172 but a full documentation of our findings is available in the **Supplementary Information**.

173 **Estradiol and between-network participation**

174 As expected, estradiol demonstrated significant autoregressive effects across all models.
175 Previous states of estradiol also significantly predicted between-network integration across
176 several intrinsic networks; however, overall model fit (variance accounted for, R^2 , and root
177 mean-squared error, $RMSE$) was at best marginal compared to empirical null distributions
178 of these statistics. For example, in the Dorsal Attention Network (DAN; **Fig. 4a-b; Table**
179 **2**), estradiol was a significant predictor of between-network participation both at lag 1 ($b =$
180 -0.56 , $SE = 0.25$, $t = -2.27$, $p = .035$) and at lag 2 ($b = 0.53$, $SE = 0.24$, $t = 2.16$, $p = .042$).
181 Overall fit for DAN participation, however, rested at the classical frequentist threshold

182 for significance, relative to empirical nulls ($R^2 = 0.32, p = .049; RMSE = 0.79, p = .050$).
183 We observed a similar pattern of results for the Default Mode Network (DMN) and
184 Limbic Network, where lagged states of estradiol significantly predicted cross-network
185 participation, but model fit as a whole was low (see **Supplementary Table 1**). Interestingly,
186 for all three of these networks, there were no significant autoregressive effects of brain
187 states—previous states of network participation also did not predict estradiol, suggesting
188 that modulation of network topology likely goes from hormones to brain, not the other
189 way around.

190 The single exception to this trend was the Visual Network. Prediction of its between-
191 network participation yielded a significant model fit ($R^2 = 0.37, p = .024; RMSE =$
192 $0.79, p = .044$). However, this was primarily driven by autoregressive effects of the
193 network at lag 1 ($b = -0.39, SE = 0.17, t = -2.30, p = .027$) and lag 2 ($b = -0.43, SE =$
194 $0.17, t = -2.46, p = .024$); estradiol yielded a marginal (but nonsignificant) effect only at
195 lag 2 ($b = 0.49, SE = 0.24, t = 2.01, p = .058$).

196 **Estradiol and global efficiency**

197 In contrast to between-network integration, estradiol was a strong predictor of within-
198 network integration, both in terms of parameter estimates and overall fit. Here, the
199 Default Mode Network provided the best-fitting model ($R^2 = 0.50, p = .003; RMSE =$
200 $0.70, p = .022$; **Fig. 5a-b**). As before, estradiol demonstrated significant autoregressive
201 effects at lag 1 ($b = 1.15, SE = 0.19, t = 6.15, p < .0001$) and lag 2 ($b = -0.48, SE =$
202 $0.19, t = -2.50, p = .012$). When predicting DMN efficiency, previous states of estradiol

203 remained significant both at lag 1 ($b = 0.98, SE = 0.23, t = 3.37, p = .0003$) and at
204 lag 2 ($b = -0.93, SE = 0.23, t = -4.00, p = .002$). Critically, these effects were purely
205 directional: prior states of Default Mode efficiency did not predict estradiol, nor did
206 they have significant autoregressive effects, supporting the conclusion that variance in
207 topological network states (perhaps within-network integration, in particular) is primarily
208 accounted for by estradiol—not the other way around (**Table 3**).

209 We observed a similar pattern of results in the Dorsal Attention Network ($R^2 =$
210 $0.37, p = .022; RMSE = 0.77, p = .023; \text{Fig. 4c; Table 3}$). Estradiol again demonstrated
211 significant autoregressive effects at lag 1 ($b = 1.17, SE = 0.19, t = 6.30, p < .0001$) and
212 lag 2 ($b = -0.48, SE = 0.19, t = -2.49, p = .011$), along with predicting DAN efficiency
213 both at lag 1 ($b = 0.84, SE = 0.25, t = 3.35, p = .002$) and at lag 2 ($b = -0.67, SE =$
214 $0.16, t = -2.57, p = .017$). As above, Dorsal Attention efficiency had no significant effects
215 on estradiol, nor were there significant autoregressive effects of the network on itself.

216 The Control and Temporal Parietal networks also yielded partial support for time-
217 dependent modulation of efficiency by estradiol (Control $R^2 = 0.34, p = .039$; Temporal
218 Parietal $R^2 = 0.36, p = .026$). The time-lagged effects of estradiol followed the trends
219 observed above; however, the overall model fit (with respect to prediction error) was not
220 significantly better than their empirical nulls (Control $RMSE = 0.83, p = .133$; Temporal
221 Parietal $RMSE = 0.79, p = .057$). Estradiol did not explain a significant proportion of
222 variance in efficiency for any other networks (see **Supplementary Table 2** for a complete
223 summary of VAR models for global efficiency).

Discussion

224

225 In this dense-sampling, deep-phenotyping project, a naturally-cycling female underwent
226 resting state fMRI and venipuncture for 30 consecutive days, capturing the dynamic
227 endocrine changes that unfold over the course of a complete menstrual cycle.
228 Time-synchronous analyses illustrate estradiol's widespread impact on cortical dynamics,
229 spanning all but one of the networks in our parcellation. Time-lagged vector
230 autoregressive models tested the temporal directionality of these effects, suggesting that
231 intrinsic network dynamics are driven by recent states of estradiol, particularly with
232 respect to within-network connectivity. Estradiol had the strongest predictive effects on
233 the efficiency of Default Mode and Dorsal Attention Networks. In contrast to estradiol's
234 proliferative effects, progesterone was primarily associated with reduced coherence across
235 the whole brain. These results reveal the rhythmic nature of brain network reorganization
236 across the human menstrual cycle.

237 The network neuroscience community has begun to probe functional networks over
238 the timescale of weeks, months, and years to understand the extent to which brain networks
239 vary between individuals or within an individual over time^{5,6,25-27}. These studies indicate
240 that functional networks are dominated by common organizational principles and stable
241 individual features, especially in frontoparietal control regions^{6,7,25,27}. An overlooked
242 feature of these regions is the dense populations of estrogen and progesterone receptors,
243 imparting exquisite sensitivity to major changes in sex hormone concentrations^{11,12,15,16,28,29}.
244 Our findings demonstrate significant effects of estradiol on functional network nodes

245 belonging to the DMN, DAN, and FCN that overlap with ER-rich regions of the brain,
246 including medial/dorsal PFC^{10,30}. This study merges the network neuroscience and
247 endocrinology disciplines by demonstrating that higher-order processing systems are
248 modulated by day-to-day changes in sex hormones over the timescale of one month.

249 Animal studies offer unambiguous evidence that sex steroid hormones shape the
250 synaptic organization of the brain, particularly in regions that support higher order
251 cognitive functions^{1,4,8,31}. In rodents, estradiol increases fast-spiking interneuron excitability
252 in deep cortical layers³¹. In nonhuman primates, whose reproductive cycle length is
253 similar to humans, estradiol increases the number of synapses in PFC³. Recently, this body
254 of work has also begun to uncover the functional significance of sinusoidal *changes* in
255 estradiol. For example, estradiol's ability to promote PFC spinogenesis in ovariectomized
256 animals occurs *only if* the hormone add-back regime mirrors the cyclic pattern of estradiol
257 release typical of the macaque menstrual cycle^{9,32}. Pairing estradiol with cyclic
258 administration of progesterone blunts this increase in spine density³². In the
259 hippocampus, progesterone has a similar inhibitory effect on dendritic spines, blocking
260 the proliferative effects of estradiol 6 hours after administration¹. Together, the preclinical
261 literature suggests that progesterone antagonizes the largely proliferative effects of
262 estradiol (for review, see Brinton and colleagues³³). We observed a similar relationship,
263 albeit at a different spatiotemporal resolution, with estradiol enhancing coherence across
264 cortical networks and progesterone diminishing it. In sum, animal studies have identified
265 estradiol's influence on regional brain organization at the microscopic scale. Here, we

266 show that estradiol and progesterone's influence is also evident at the mesoscopic scale of
267 whole-brain activation, measured by spectral coherence, and macroscopic features of
268 network topology.

269 Additional evidence from group-based or sparser-sampling neuroimaging studies
270 provide further support that cycle stage and sex hormones impact resting state
271 networks¹³¹⁴. Arélin and colleagues³⁴ sampled an individual every 2-3 days across four
272 cycles and found that progesterone was associated with increased connectivity between
273 the hippocampus, dorsolateral PFC and the sensorimotor cortex, providing compelling
274 evidence that inter-regional connectivity varies over the cycle. However, the sampling rate
275 of this correlational study precluded the authors from capturing the neural effects of
276 day-to-day changes in sex steroid hormones and from testing the temporal directionality
277 of the effect with time-lagged models. Estradiol has both rapid, non-genomic effects and
278 slower, genomic effects on the central nervous system. For example, over the rat estrous
279 cycle, there is a dramatic 30% increase in hippocampal spine density within the 24-hour
280 window in which estradiol concentrations peak. Here, we sought to capture both
281 time-synchronous (rapid) and time-lagged (delayed) effects of sex steroid hormones,
282 sampling every 24 hours for 30 consecutive days. In contrast to Arélin and colleagues, we
283 observed robust, spatially-diffuse negative relationships between progesterone and
284 coherence across the brain, while estradiol enhanced the global efficiency of discrete
285 networks along with between-network integration. Our results illuminate how
286 simultaneous, time-synchronous correlations and causal, time-lagged analysis reveal

287 unique aspects of where and how hormones exert their effect on the brain's intrinsic
288 networks: time synchronous analyses illustrate estrogen and progesterone's widespread
289 influence on cortical coupling, while vector autoregressive models allowed us to examine
290 the temporal flow of effect in those relationships, showing that estradiol *drives* increased
291 connectivity—particularly in DMN and DAN.

292 The following considerations could enhance the interpretation of these data. First,
293 this study represents extensive neural phenotyping of a healthy participant with canonical
294 hormone fluctuations over a reproductive cycle. To enrich our understanding of the
295 relationship between sex hormones and brain function, examining network organization in
296 a hormonally-suppressed female (i.e. an oral contraceptive user) would serve as a valuable
297 comparison. Oral hormonal contraceptives suppress the production of ovarian hormones:
298 if dynamic changes in estradiol are indeed *causing* increases in resting connectivity, we
299 expect hormonally-suppressed individuals to show blunted functional brain network
300 dynamics over time. Given the widespread use of oral hormonal contraceptives (100
301 million users worldwide), it is critical to determine whether sweeping changes to an
302 individual's endocrine state impacts brain states and whether this, in turn, has any bearing
303 on cognition.

304 Second, in normally-cycling individuals, sex hormones function as
305 proportionally-coupled *nonlinear* oscillators³⁵. Within-person cycle variability is almost as
306 large as between-person cycle variability, which hints that there are highly-complex
307 hormonal interactions within this regulatory system^{35,36}. The VAR models we have

308 explored reveal linear dependencies between brain states and hormones, but other
309 dynamical systems methods (e.g. coupled latent differential equations) may offer more
310 biophysical validity³⁵. Unfortunately, the current sample of only one individual across
311 one complete cycle precludes robust estimation of such a model. Future studies should
312 enroll a larger sample of women to assess whether individual differences in hormone
313 dynamics drive network changes.

314 Third, while coherence is theoretically robust to timing differences in the
315 hemodynamic response function, hormones can affect the vascular system³⁷. Therefore,
316 changes in coherence may be due to vascular artifacts that affect the hemodynamic
317 response in fMRI, rather than being *neurally*-relevant. Future investigations exploring the
318 assumptions of hemodynamics in relation to sex steroid hormone concentrations will add
319 clarity as to how the vascular system's response to hormones might influence large-scale
320 brain function.

321 Fourth, these findings contribute to an emerging body of work on estradiol's ability
322 to enhance the efficiency of PFC-based cortical circuits. In young women performing a
323 working memory task, PFC activity is exaggerated under low estradiol conditions and
324 reduced under high estradiol conditions¹². The same pattern is observed decades later in
325 life: as estradiol production decreases over the menopausal transition, working memory-
326 related PFC activity becomes more exaggerated, despite no difference in working memory
327 performance¹⁵. Here, we show that day-to-day changes in estradiol drive the global
328 efficiency of functional networks, with the most pronounced effects in networks with

329 major hubs in the PFC. Together, these findings suggest that estradiol generates a neurally
330 efficient PFC response at rest and while engaging in a cognitive task. The mechanism by
331 which this occurs may be through enhancing dopamine synthesis and release³⁸: the PFC
332 is innervated by midbrain dopaminergic neurons that form the mesocortical dopamine
333 track³⁹. Decades of evidence have established that dopamine signaling enhances the signal-
334 to-noise ratio of PFC pyramidal neurons⁴⁰ and drives cortical efficiency⁴¹⁻⁴⁴. More recently
335 it was discovered that estradiol enhances dopamine synthesis, release, and turnover and
336 modifies the basal firing rate of dopaminergic neurons⁴⁵⁻⁴⁷, a plausible neurobiological
337 mechanism by which alterations in estradiol could impact cortical efficiency. Future
338 multimodal neuroimaging studies in humans can clarify the link between estradiol's
339 ability to stimulate dopamine release and the hormone's ability to drive cortical efficiency
340 within PFC circuits.

341 Using dense-sampling approaches to probe brain-hormone interactions could reveal
342 organizational principles of the functional connectome previously unknown, transforming
343 our understanding of how hormones influence brain states. Human studies implicate
344 sex steroids in the regulation of brain structure and function, particularly within ER-rich
345 regions like the PFC and hippocampus^{11,12,15,16,28,29,48,50}, yet the neuroendocrine basis of the
346 brain's network organization remains understudied. A network neuroscience approach
347 allows us to understand how hormones modulate the integration of functional brain
348 networks that span the entire cortical surface and subcortex, as opposed to examining
349 discrete brain regions in isolation. Using this approach, we show that estradiol is associated

350 with increased coherence across broad swaths of cortex. At the network level, estradiol
351 enhances the efficiency of most functional networks (with robust effects in DAN and DMN)
352 and, to a lesser extent, increases between-network participation. Moving forward, this
353 network neuroscience approach can be applied to brain imaging studies of other major
354 neuroendocrine transitions, such as pubertal development and reproductive aging (e.g.
355 menopause).

356 An overarching goal of network neuroscience is to understand how coordinated
357 activity within and between functional brain networks supports cognition. Increased
358 global efficiency is thought to optimize a cognitive workspace⁵¹, while between-network
359 connectivity may be integral for integrating top-down signals from multiple higher-order
360 control hubs⁵². The dynamic reconfiguration of functional brain networks is implicated in
361 performance across cognitive domains, including motor learning^{53,54}, cognitive control⁵⁵,
362 and memory⁵⁶. Our results demonstrate that within- and between-network connectivity
363 of these large-scale networks at rest are hormonally regulated across the human menstrual
364 cycle. Future studies should consider whether these network changes confer advantages to
365 domain-general or domain-specific cognitive performance. Further, planned analyses from
366 this dataset will incorporate task-based fMRI to determine whether the brain's network
367 architecture is hormonally regulated across the cycle when engaging in a cognitive task, or
368 in the dynamic reconfiguration that occurs when transitioning from rest to task.

369 The emerging field of clinical network neuroscience also seeks to understand how
370 large-scale brain networks differ between healthy and patient populations^{57,58}.

371 Disruptions in functional brain networks are implicated in a number of neurodegenerative
372 and neuropsychiatric disorders. For example, intrinsic connectivity abnormalities in the
373 DMN are evident in major depressive disorder⁵⁹ and Alzheimer's disease⁶⁰. Notably,
374 these conditions have a sex-skewed disease prevalence: women are at twice the risk for
375 depression and make up two-thirds of the Alzheimer's disease patient population⁶¹. Here,
376 we show that global efficiency in the DMN and DAN are hormonally regulated, with
377 estradiol driving increases in within-network integration. A long history of clinical
378 evidence further implicates sex hormones in the development of mood disorders^{62,63}.
379 Throughout the lifecourse, changes in women's reproductive status have been associated
380 with increased risk for depression⁶⁴⁻⁶⁷. For example, the incidence of major depression
381 increases with pubertal onset in females⁶⁸, chronic use of hormonal contraceptives⁶⁹, the
382 postpartum period⁷⁰, and perimenopause⁷¹. Moving forward, a network neuroscience
383 approach could identify the large-scale network disturbances that underlie, or predict, the
384 emergence of disease symptomology. Incorporating sex-dependent variables (such as
385 endocrine status) into clinical network neuroscience models may be essential for
386 identifying individuals at risk of disease. This may be particularly true during periods of
387 profound neuroendocrine change (e.g. puberty, pregnancy, menopause, and use of
388 hormone-based medications, reviewed by Taylor and colleagues⁷²) given that these
389 hormonal transitions are associated with a heightened risk for mood disorders.

390 In sum, endogenous hormone fluctuations over the reproductive cycle have a robust
391 impact on the intrinsic network properties of the human brain. Despite over 20 years of

392 evidence from rodent, nonhuman primate, and human studies demonstrating the tightly-
393 coupled relationship between our endocrine and nervous systems, the field of network
394 neuroscience has largely overlooked how endocrine factors shape the brain. The dynamic
395 endocrine changes that unfold over the menstrual cycle are a natural feature of half of
396 the world's population. Understanding how these changes in sex hormones influence
397 the large-scale functional architecture of the human brain is imperative for our basic
398 understanding of the brain and for women's health.

End Notes

399

400 **Acknowledgements.** This work was supported by the Brain and Behavior Research
401 Foundation (EGJ), the California Nanosystems Institute (EGJ), the Institute for
402 Collaborative Biotechnologies through grant W911NF-19-D-0001 from the U.S. Army
403 Research Office (MBM), and the Rutherford B. Fett Fund (SG). Thanks to Mario Mendoza
404 for phlebotomy and MRI assistance. We would also like to thank Courtney Kenyon,
405 Maggie Hayes, and Morgan Fitzgerald for assistance with data collection.

406 **Author contributions.** The overall study was conceived by L.P., C.M.T., and E.G.J.;
407 L.P., T.S., E.L., C.M.T., S.Y., and E.G.J. performed the experiments; data analysis strategy
408 was conceived by T.S. and L.P. and implemented by T.S.; L.P., T.S., and E.G.J. wrote the
409 manuscript; E.L., C.M.T., S.Y., M.B.M., and S.T.G. edited the manuscript.

410 **Data/code availability.** MRI data, code, and daily behavioral assessments will be
411 publicly accessible upon publication.

412 **Conflict of interest.** The authors declare no competing financial interests.

Online Methods

413

414 **Participants**

415 The participant (author L.P.) was a right-handed Caucasian female, aged 23 years for
416 duration of the study. The participant had no history of neuropsychiatric diagnosis,
417 endocrine disorders, or prior head trauma. She had a history of regular menstrual cycles
418 (no missed periods, cycle occurring every 26-28 days) and had not taken hormone-based
419 medication in the prior 12 months. The participant gave written informed consent and
420 the study was approved by the University of California, Santa Barbara Human Subjects
421 Committee.

422 **Study design**

423 The participant underwent daily testing for 30 consecutive days, with the first test session
424 determined independently of cycle stage for maximal blindness to hormone status. The
425 participant began each test session with a daily questionnaire (see **Behavioral assessment**),
426 followed by an immersive reality spatial navigation task (not reported here) (**Fig. 6**).
427 Time-locked collection of serum and whole blood started each day at 10:00am, when the
428 participant gave a blood sample. Endocrine samples were collected, at minimum, after
429 two hours of no food or drink consumption (excluding water). The participant refrained
430 from consuming caffeinated beverages before each test session. The MRI session lasted
431 one hour and consisted of structural and functional MRI sequences.

432 Behavioral assessments

433 To monitor state-dependent mood and lifestyle measures over the cycle, the following
434 scales (adapted to reflect the past 24 hours) were administered each morning: Perceived
435 Stress Scale (PSS)⁷³, Pittsburgh Sleep Quality Index (PSQI)⁷⁴, State-Trait Anxiety Inventory
436 for Adults (STAI)⁷⁵, Profile of Mood States (POMS)⁷⁶, and the Sexual Desire Inventory-2
437 (SDI-2)⁷⁷. We observed very few significant relationships between hormone and state-
438 dependent measures following an FDR-correction for multiple comparisons ($q < .05$)—and
439 critically, none of these state-dependent factors were associated with estradiol (**Fig. 7a**).
440 The participant had moderate levels of anxiety as determined by STAI reference ranges;
441 however, all other measures fell within the ‘normal’ standard range (**Fig. 7b**).

442 Endocrine procedures

443 A licensed phlebotomist inserted a saline-lock intravenous line into the dominant or
444 non-dominant hand or forearm daily to evaluate hypothalamic-pituitary-gonadal axis
445 hormones, including serum levels of gonadal hormones (17β -estradiol, progesterone and
446 testosterone) and the pituitary gonadotropins luteinizing hormone (LH) and follicle
447 stimulating hormone (FSH). One 10cc mL blood sample was collected in a vacutainer SST
448 (BD Diagnostic Systems) each session. The sample clotted at room temperature for 45 min
449 until centrifugation ($2,000 \times g$ for 10 minutes) and were then aliquoted into three 1 ml
450 microtubes. Serum samples were stored at -20° C until assayed. Serum concentrations
451 were determined via liquid chromatography-mass spectrometry (for all steroid hormones)

452 and immunoassay (for all gonadotropins) at the Brigham and Women's Hospital Research
453 Assay Core. Assay sensitivities, dynamic range, and intra-assay coefficients of variation
454 (respectively) were as follows: estradiol, 1 pg/mL, 1–500 pg/mL, < 5% relative standard
455 deviation (*RSD*); progesterone, 0.05 ng/mL, 0.05–10 ng/mL, 9.33% *RSD*; testosterone, 1.0
456 ng/dL, 1–2000 ng/dL, < 4% *RSD*; FSH and LH levels were determined via
457 chemiluminescent assay (Beckman Coulter). The assay sensitivity, dynamic range, and the
458 intra-assay coefficient of variation were as follows: FSH, 0.2 mIU/mL, 0.2–200 mIU/mL,
459 3.1–4.3%; LH, 0.2 mIU/mL, 0.2–250 mIU/mL, 4.3–6.4%.

460 **fMRI acquisition and preprocessing**

461 The participant underwent a daily magnetic resonance imaging scan on a Siemens 3T
462 Prisma scanner equipped with a 64-channel phased-array head coil. First, high-resolution
463 anatomical scans were acquired using a T_1 -weighted magnetization prepared rapid
464 gradient echo (MPRAGE) sequence (TR = 2500 ms, TE = 2.31 ms, TI = 934 ms, flip angle =
465 7° ; 0.8 mm thickness) followed by a gradient echo fieldmap (TR = 758 ms, TE₁ = 4.92 ms,
466 TE₂ = 7.38 ms, flip angle = 60°). Next, the participant completed a 10-minute resting-state
467 fMRI scan using a T_2^* -weighted multiband echo-planar imaging (EPI) sequence sensitive
468 to the blood oxygenation level-dependent (BOLD) contrast (TR = 720 ms, TE = 37 ms, flip
469 angle = 56° , multiband factor = 8; 72 oblique slices, voxel size = 2 mm³). In an effort to
470 minimize motion, the head was secured with a custom, 3D-printed foam head case
471 (<https://caseforge.co/>) (days 8-30). Overall motion (mean framewise
472 displacement) was negligible (**Supplementary Fig. 3**), with fewer than 130 microns of

473 motion on average each day. Importantly, mean framewise displacement was also not
474 correlated with estradiol concentrations (Spearman $r = -0.06, p = .758$).

475 Initial preprocessing was performed using the Statistical Parametric Mapping 12
476 software (SPM12, Wellcome Trust Centre for Neuroimaging, London) in Matlab.
477 Functional data were realigned and unwarped to correct for head motion and the mean
478 motion-corrected image was coregistered to the high-resolution anatomical image. All
479 scans were then registered to a subject-specific anatomical template created using
480 Advanced Normalization Tools (ANTs) multivariate template construction
481 (**Supplementary Fig. 4**). A 5 mm full-width at half-maximum (FWHM) isotropic
482 Gaussian kernel was subsequently applied to smooth the functional data. Further
483 preparation for resting-state functional connectivity was implemented using in-house
484 Matlab scripts. Global signal scaling (median = 1,000) was applied to account for
485 fluctuations in signal intensity across space and time, and voxelwise timeseries were
486 linearly detrended. Residual BOLD signal from each voxel was extracted after removing
487 the effects of head motion and five physiological noise components (CSF + white matter
488 signal). Motion was modeled based on the Friston-24 approach, using a Volterra
489 expansion of translational/rotational motion parameters, accounting for autoregressive
490 and nonlinear effects of head motion on the BOLD signal^[78]. All nuisance regressors were
491 detrended to match the BOLD timeseries.

492 **Functional connectivity estimation**

493 Functional network nodes were defined based on a 400-region cortical parcellation²⁴
494 and 15 regions from the Harvard-Oxford subcortical atlas ([http://www.fmrib.ox.
495 ac.uk/fsl/](http://www.fmrib.ox.ac.uk/fsl/)). For each day, a summary timecourse was extracted per node by taking
496 the first eigenvariate across functional volumes⁷⁹. These regional timeseries were then
497 decomposed into several frequency bands using a maximal overlap discrete wavelet
498 transform. Low-frequency fluctuations in wavelets 3–6 (~0.01–0.17 Hz) were selected
499 for subsequent connectivity analyses⁸⁰. Finally, we estimated the spectral association
500 between regional timeseries using magnitude-squared coherence: this yielded a 415×415
501 functional association matrix each day, whose elements indicated the strength of functional
502 connectivity between all pairs of nodes (FDR-thresholded at $q < .05$).

503 **Statistical analysis**

504 First, we assessed time-synchronous variation in functional connectivity associated with
505 estradiol and progesterone through a standardized regression analysis. Data were Z -
506 transformed and edgewise coherence was regressed against hormonal timeseries to capture
507 day-by-day variation in connectivity relative to hormonal fluctuations. For each model,
508 we computed robust empirical null distributions of test-statistics via 10,000 iterations of
509 nonparametric permutation testing—while this process has been shown to adequately
510 approximate false positive rates of 5%⁸¹, we elected to report only those edges surviving a
511 conservative threshold of $p < .001$ to avoid over-interpretation of whole-brain effects.

512 Next, we sought to capture *causal* linear dependencies between estradiol and network
 513 connectivity over time using vector autoregressive (VAR) models. A given VAR model
 514 takes a set of variables at time, t , and simultaneously regresses them against previous
 515 (time-lagged) states of themselves and each other. For consistency, we only considered
 516 second-order VAR models, given a fairly reliable first zero-crossing of brain/hormone
 517 autocovariance functions at lag two. Fit parameters for each VAR therefore reflect the
 518 following general form:

$$\begin{aligned}
 Brain_t &= b_{1,0} + b_{1,1}Brain_{t-1} + b_{1,2}Estradiol_{t-1} + b_{1,3}Brain_{t-2} + b_{1,4}Estradiol_{t-2} + e_t \\
 Estradiol_t &= b_{2,0} + b_{2,1}Brain_{t-1} + b_{2,2}Estradiol_{t-1} + b_{2,3}Brain_{t-2} + b_{2,4}Estradiol_{t-2} + e_t
 \end{aligned}
 \tag{1}$$

519 With respect to brain states, we modeled both edgewise coherence and factors related
 520 to macroscale network topologies. Specifically, we computed measures of *between-network*
 521 integration (the participation coefficient; i.e. the average extent to which network nodes
 522 are communicating with other networks over time) and *within-network* integration (global
 523 efficiency, quantifying the ostensible ease of information transfer across nodes inside
 524 a given network). Regardless of brain measure, each VAR was estimated similarly to
 525 the time-synchronous analyses described above: data were Z -scored, models were fit,
 526 and all effects were empirically-thresholded against 10,000 iterations of nonparametric
 527 permutation testing.

528 Finally, for each set of edgewise models (time-synchronous and time-lagged), we
 529 attempted to disentangle both the general *direction* of hormone-related associations and

530 whether certain networks were more or less *susceptible* to hormonal fluctuations. Toward
531 that end, we estimated *nodal association strengths* per graph theory's treatment of signed,
532 weighted networks—that is, positive and negative association strengths were computed
533 independently for each node by summing the positive and negative edges linked to them
534 (after empirical thresholding), respectively. We then simply assessed mean association
535 strengths across the various networks in our parcellation.

536 Here, networks were defined by grouping the subnetworks of the 17-network Schaefer
537 parcellation, such that (for example), the A, B, and C components of the Default Mode
538 Network were treated as one network. We chose this due to the presence of a unique
539 Temporal Parietal Network in the 17-network partition, which is otherwise subsumed
540 by several other networks (Default Mode, Ventral Attention, and SomatoMotor) in the
541 7-network partition. The subcortical nodes of the Harvard-Oxford atlas were also treated as
542 their own network, yielding a total of nine networks. These definitions were subsequently
543 used for computation of participation coefficients and global efficiencies in network-level
544 VAR models.

545 **Brain data visualization**

546 Statistical maps of edgewise coherence v. hormones were visualized using the Surf Ice
547 software (<https://www.nitrc.org/projects/surface/>).

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Table 1. Gonadal and pituitary hormones by cycle stage.

	Follicular	Ovulatory	Luteal
	Mean (SD) <i>standard range</i>	Mean (SD) <i>standard range</i>	Mean (SD) <i>standard range</i>
Estradiol (pg/mL)	37.9 (15.9) 12.5-166.0	185.3 (59.0) 85.8-498.0	85.4 (26.4) 43.8-210.0
Progesterone (ng/mL)	0.2 (0.2) 0.1-0.9	0.2 (.2) 0.1-120	9.5 (4.8) 1.8-23.9
LH (mIU/mL)	5.9 (0.7) 2.4-12.6	21.7 (16.4) 14.0-95.6	5.5 (2.0) 1.0-11.4
FSH (mIU/mL)	6.5 (1.2) 3.5-12.5	8.1 (3.6) 4.7-21.5	4.8 (1.3) 1.7-7.7

Note. Standard reference ranges based on aggregate data from Labcorp
[\(https://www.labcorp.com/\)](https://www.labcorp.com/)

Table 2. Vector autoregressive model for cross-network participation.

Network	Outcome	Predictor	Estimate	SE	T (p)
		Constant	0.08	0.16	0.49 (.099)
		DAN _{t-1}	0.15	0.18	0.84 (.405)
	Participation	Estradiol_{t-1}	-0.56	0.25	-2.27 (.035)
		DAN _{t-2}	-0.29	0.17	-1.71 (.093)
		Estradiol_{t-2}	0.53	0.24	2.16 (.042)
		R² = 0.32 (p = .049); RMSE = 0.79 (p = .050)			
<i>Dorsal Attention</i>		Constant	6.88 x 10 ⁻⁵	0.12	0.001 (.998)
		DAN _{t-1}	0.06	0.14	0.47 (.627)
	Estradiol	Estradiol_{t-1}	1.12	0.18	6.12 (< .0001)
		DAN _{t-2}	0.03	0.13	0.24 (.806)
		Estradiol_{t-2}	-0.48	0.18	-2.65 (.007)
		R² = 0.67 (p = .0001); RMSE = 0.59 (p = .0009)			

Note. p-values empirically-derived via 10,000 iterations of nonparametric permutation testing.

Table 3. Vector autoregressive models for global efficiency.

Network	Outcome	Predictor	Estimate	SE	T (p)	
Default Mode	Efficiency	Constant	0.04	0.15	0.28 (.279)	
		DMN _{t-1}	-0.04	0.16	-0.27 (.764)	
		Estradiol_{t-1}	0.98	0.23	3.37 (.0003)	
		DMN _{t-2}	-0.02	0.16	-0.11 (.907)	
		Estradiol_{t-2}	-0.93	0.23	-4.00 (.002)	
	R² = 0.50 (p = .003); RMSE = 0.70 (p = .022)					
	Estradiol	Constant	0.01	0.12	0.09 (.729)	
		DMN _{t-1}	-0.12	0.13	-0.95 (.339)	
		Estradiol_{t-1}	1.15	0.19	6.15 (< .0001)	
		DMN _{t-2}	-0.01	0.13	-0.08 (.930)	
Estradiol_{t-2}		-0.48	0.19	-2.50 (.012)		
R² = 0.67 (p < .0001); RMSE = 0.58 (p = .0004)						
Dorsal Attention	Efficiency	Constant	0.01	0.16	0.08 (.783)	
		DAN _{t-1}	-0.11	0.18	-0.60 (.562)	
		Estradiol_{t-1}	0.84	0.25	3.35 (.002)	
		DAN _{t-2}	-0.10	0.18	-0.58 (.571)	
		Estradiol_{t-2}	-0.67	0.16	-2.57 (.017)	
	R² = 0.37 (p = .022); RMSE = 0.77 (p = .023)					
	Estradiol	Constant	0.01	0.12	0.06 (.808)	
		DAN _{t-1}	-0.17	0.13	-1.29 (.207)	
		Estradiol_{t-1}	1.17	0.19	6.30 (< .0001)	
		DAN _{t-2}	-0.02	0.13	-0.16 (.875)	
Estradiol_{t-2}		-0.48	0.19	-2.49 (.011)		
R² = 0.68 (p < .0001); RMSE = 0.57 (p = .0004)						

Note. p-values empirically-derived via 10,000 iterations of nonparametric permutation testing.

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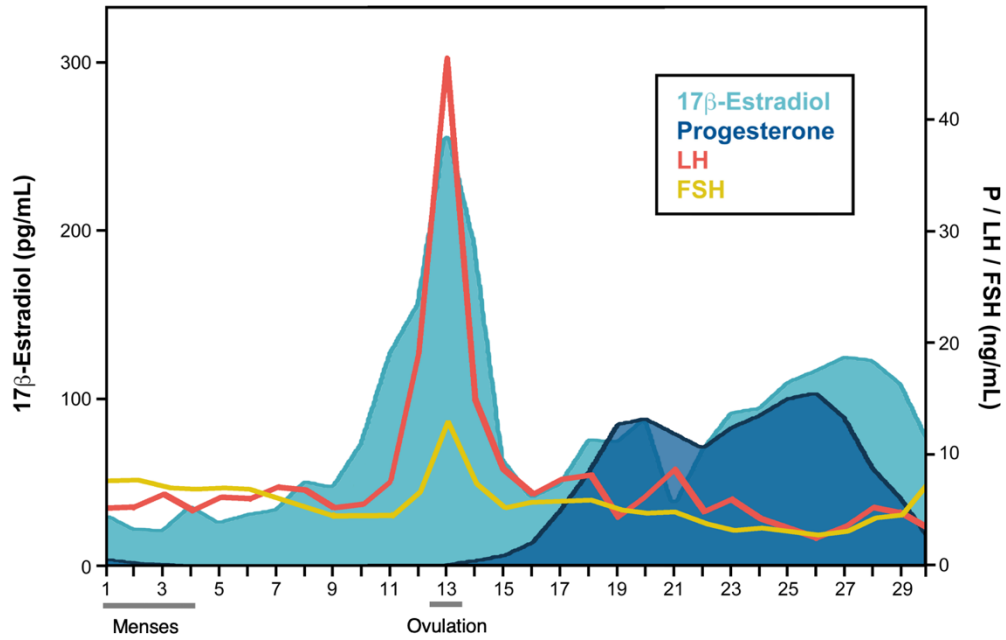


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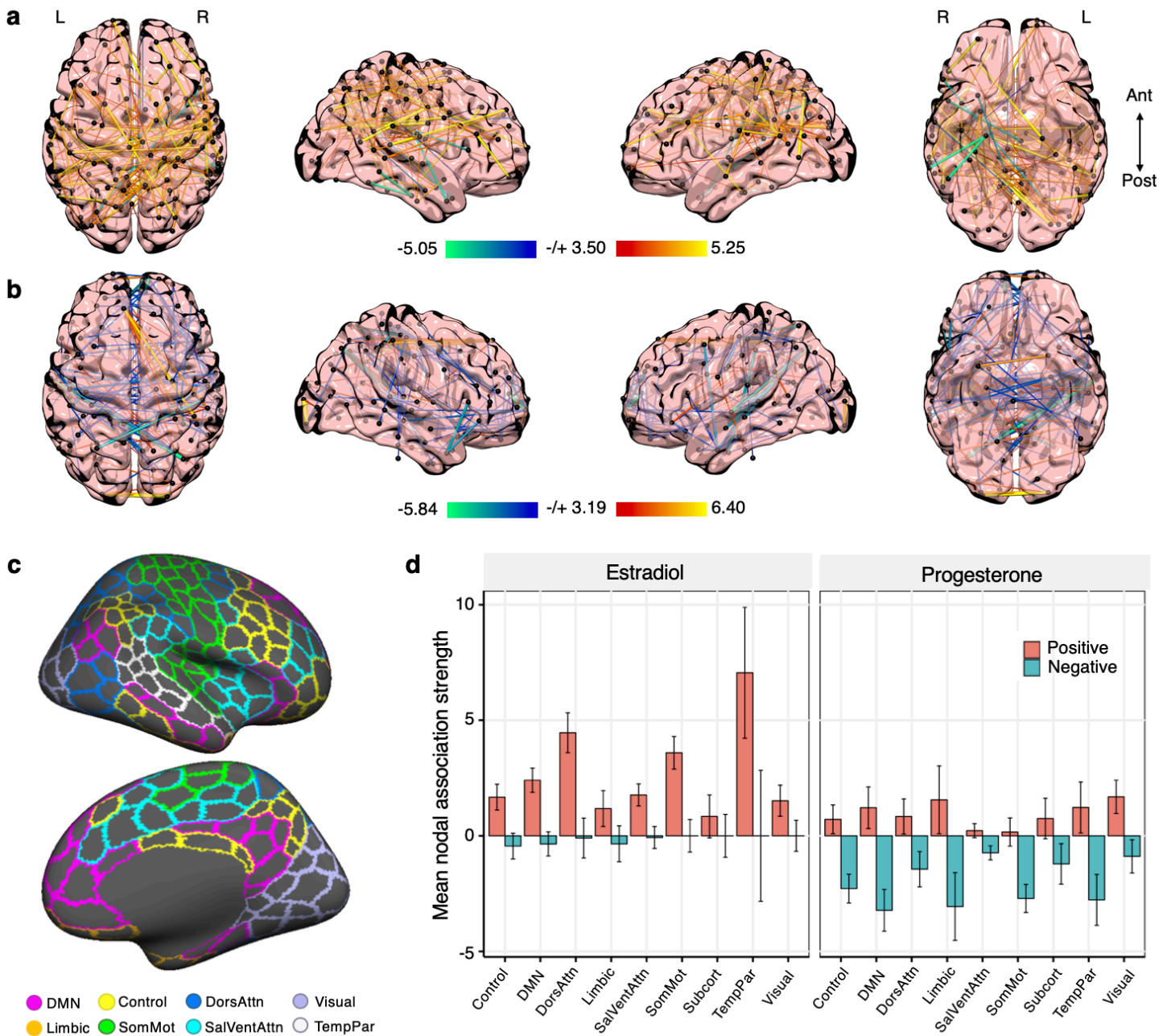


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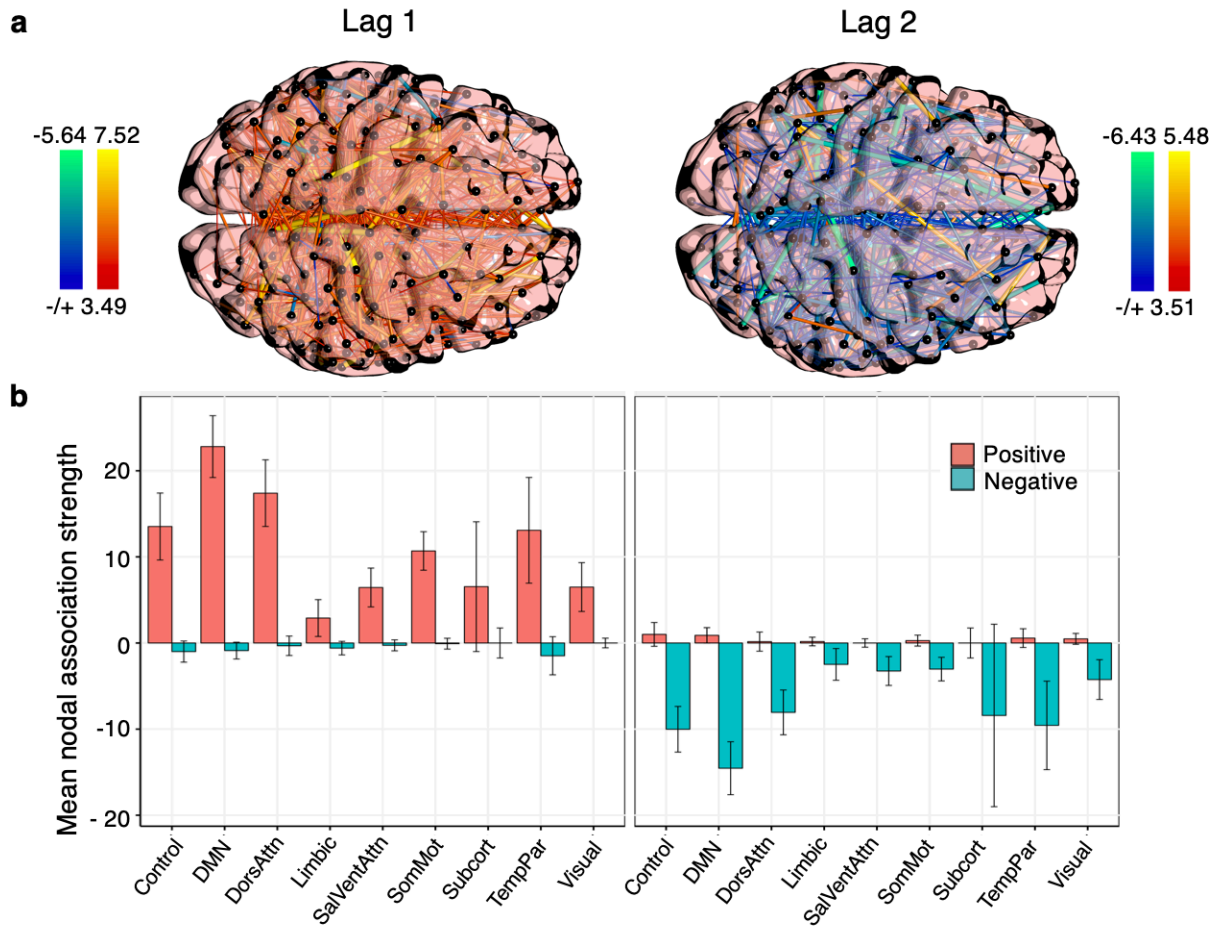


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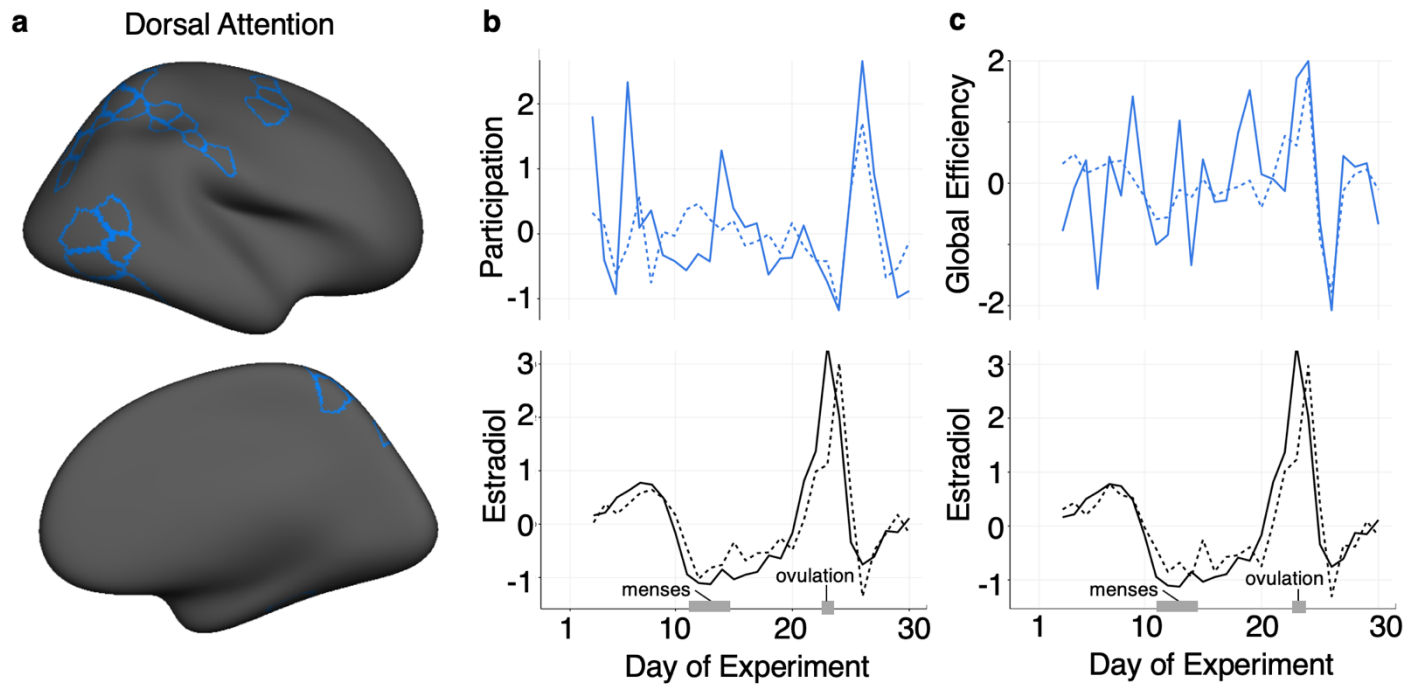


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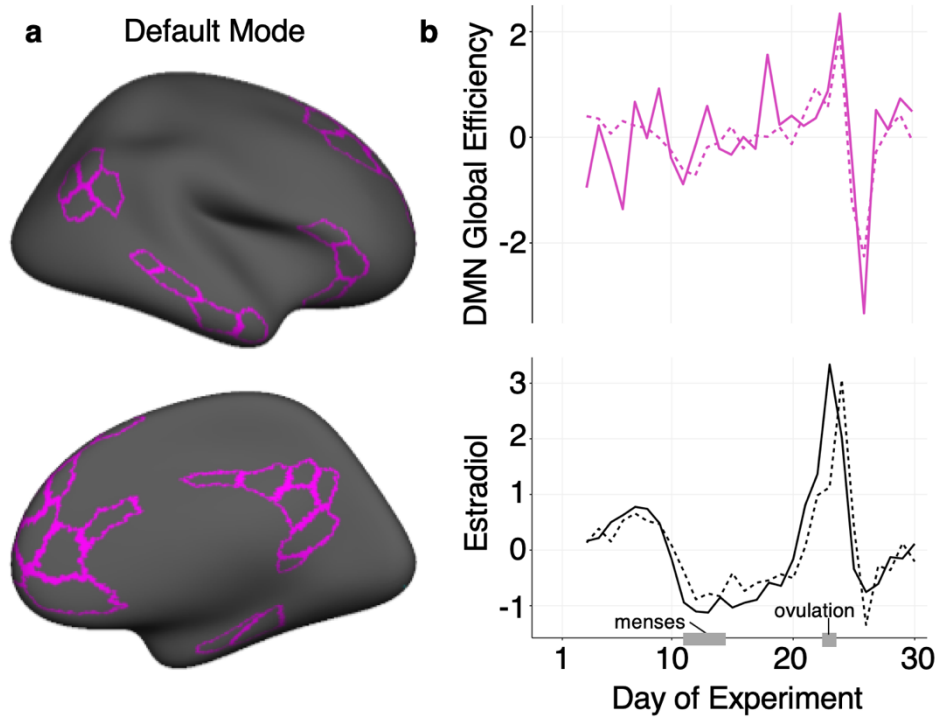


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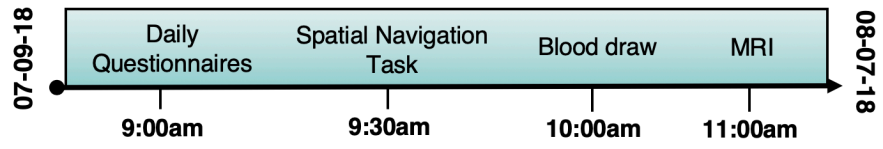


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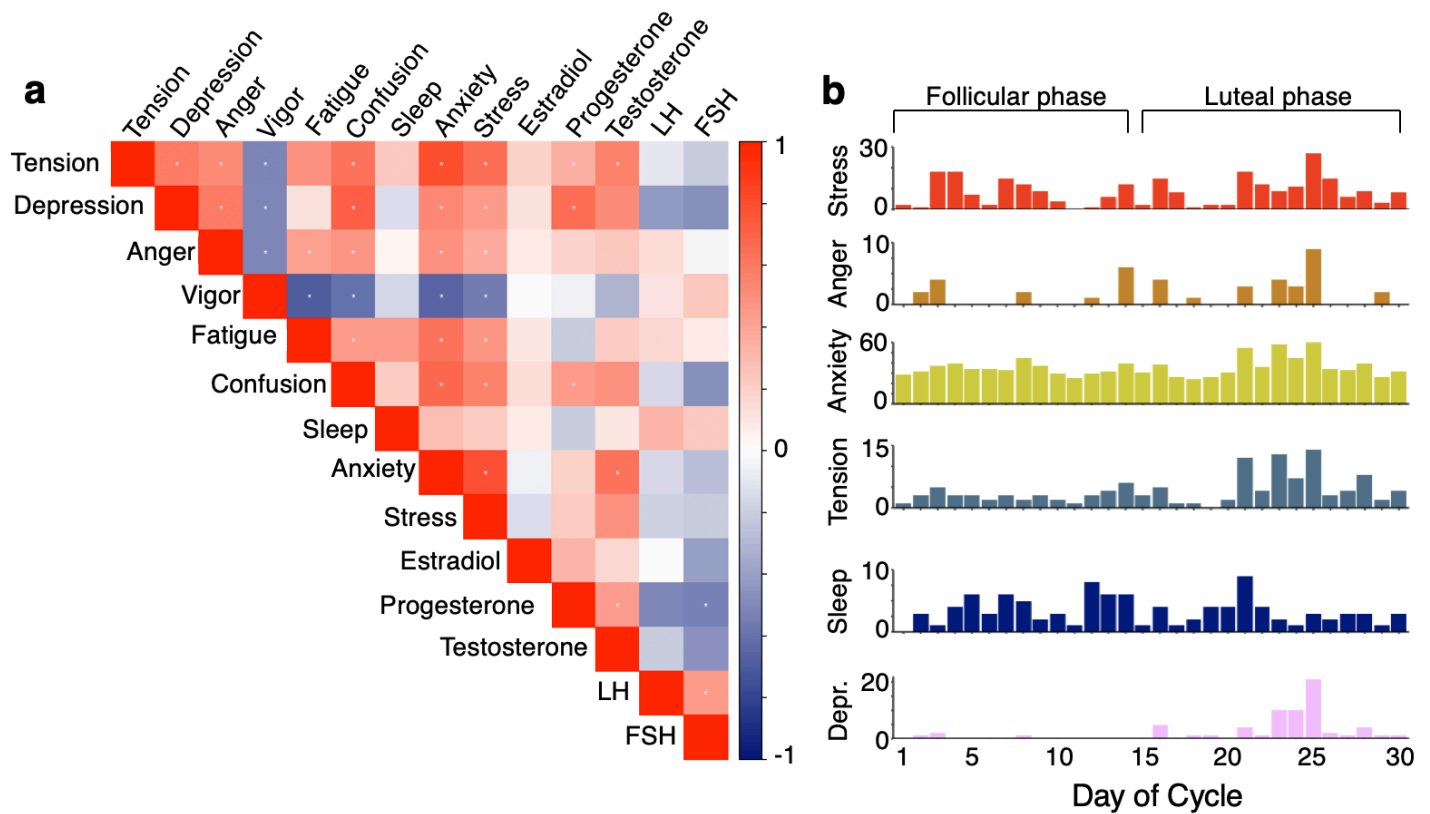


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